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NanowireSensor **RTD2009**



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Sensing with Silicon Nanowire Field-Effect Transistors

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Silicon nanowire FETs as sensing units

Small semiconductor FETs such as silicon nanowires can serve as sensing units in integrateable bio- and chemical sensors.¹⁻³ Charged species at the nanowire surface can lead to depletion or accumulation of carriers in the FET channel, modulating its conductance.

The nanowire arrays are fabricated in a SOI wafer. Gate voltage is applied via the silicon substrate below. In solution, an additional gate voltage can be applied via a Pt electrode (dual-gating).³⁻⁵

A calomel reference electrode measures the effective liquid potential.



Main Achievements:

- > Routine operation of NW arrays;
- > Various surface modification schemes;
- > Understanding of pH and electrolyte effects;
- > Differential measurements;
- > Specific ion sensing.

Fabrication of nanowire arrays

Summary of the top-down fabrication process:

Device structuring: 48 NWs are defined by e-beam lithography on a SOI wafer. Dry and wet etching to shape the NWs.

Ohmic contacts: contact areas are heavily doped by ion implantation and annealing. Aluminum pads are evaporated ¹ and annealed for optimal contact.

ALD interface oxide: the whole device is coated with a thin AI_2O_3 or HfO_2 layer (a) to prevent leakage currents and (b) to optimize sensing properties

Packaging: micro-channels are defined in SU-8, sample is wire-bonded into chip carrier, and sealed with epoxy.







pH sensing and electrolyte effects⁶

Close to ideal pH sensitivity: Conductance G of a NW vs. liquid potential at different pH values. The threshold voltage shift is read out in the subthreshold regime and plotted vs. pH (inset). According to the Bergveld model, this shift is described by

 $\Delta V_{th} = \ln(10)kT/e \cdot \alpha \cdot \Delta pH$, where

$\alpha = C_s / (C_d + C_s) \le 1.$

C_d: double-layer capacitance C_s: surface buffer capacitance

The observed pH response is very close to the ideal Nernstian value of In(10)*kT/e* ≈ 59.5 mV/pH at RT (α≈1).

Negligible electrolyte effect at c < 10 mM: Varying the ionic strength changes C_a. However, almost no potential change is visible, since the sensitivity parameter $\alpha \approx 1$





The pH response ΔV of several samples was tested, showing a **decrea**sing pH sensitivity with increasing surface coverage.

The site-binding model (SBM, lines) was used to fit the data (squares). The number of surface sites N was extracted from the fits.

A reduction of N by three orders of magnitude is achieved after 7 days, resulting in a **pH insensitive** surface.

Vapor deposition of a silane with a long alkyl chain (C18) was used to passivate the Al₂O₃ surface. Contact angle (CA) was measured to get some information on the reaction progress.



We define an average pH sensitivity

 $s_{pH} = \Delta V_{max} / (pH_{sat2} - pH_{sat1})$ and plot

it together with N_s. Both quantities

Fully passivated NW could be used

N_c[cm

8

were taken from the above plot.

as **pH reference** electrodes.

0.1

-0.1



Ion sensing in a differential setup







Partially passivated surface is sensitive to δN_s , caused by adsorption of neutral species. ¥

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Define sensitivity S = \delta \Psi_0 / \delta N_s.
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Estimated detection limit: δN ≈ 170 μm⁻²Hz^{-1/2} (at 10 Hz, pH = 3)

Partners:



References:

 $10^{14} N_{s}[cm^{-2}]$

6

рH

.10¹³

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pK_a=pK_b=7

10

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